A Review Study for Electrocardiogram Signal Classification



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ABSTRACT

An electrocardiogram (ECG) signal is a recording of the electrical activity generated by the heart. The analysis of the ECG signal has been interested in more than a decade to build a model to make automatic ECG classification. The main goal of this work is to study and review an overview of utilizing the classification methods that have been recently used such as Artificial Neural Network, Convolution Neural Network (CNN), discrete wavelet transform, Support Vector Machine (SVM), and K-Nearest Neighbor. Efficient comparisons are shown in the result in terms of classification methods, features extraction technique, dataset, contribution, and some other aspects. The result also shows that the CNN has been most widely used for ECG classification as it can obtain a higher success rate than the rest of the classification approaches.

Index Terms: Artificial neural network, Convolution neural network, Discrete wavelet transform, Support vector machine, K-nearest neighbor

1. INTRODUCTION

An electrocardiogram (ECG) is simply a recording of the electrical activity generated by the heart [1]. The heart produces the electrical activity that measures by a medical test called an ECG, which identifies the cardiac abnormality [2]. A heart produces tiny electrical impulses that spread through the heart muscle [3]. An ECG all data about the electrical activity of the heart records and shows on a paper by an ECG machine [4]. Then, a medical practitioner interprets this data; ECG leads to find the cause of symptoms of chest pain and also leads to detect abnormal heart rhythm [5].

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An ECG signal has a total of five primary turns, counting P, Q, R, S, and T waves, plus the depolarization of the atria causes a small turn before atria contraction as the activation (depolarization) wave-front propagates from the Sino atria node through the atria [6]. The Q wave is a downward deflection after the P wave [7]. The R wave follows as an upward deflection, and the S wave is a downward deflection following the R wave [8]. Q, R, and S waves together indicate a single event [9]. Hence, they are usually considered to be QRS complex, as shown in Fig. 1 [10], [11].

The features based on the QRS complex are among the most powerful features for ECG analysis [13]. The QRS-complex is caused by currents that are generated when the ventricles depolarize before their contraction [14]. Although atrial depolarization occurs before ventricular depolarization, the latter waveform (i.e., the QRS-complex) has much higher amplitude, and atria depolarization is, therefore, not seen on an ECG. The T wave, which follows the S wave, is ventricular depolarization, where the heart muscle prepares for the next

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ECG cycle [15]. Finally, the U wave is a small deflection that immediately follows the T wave. The U wave is usually in the same direction as the T wave [16].

There are different kinds of arrhythmias, and each kind is associated with a pattern, and as such, it is possible to recognize and classify it [17]. The arrhythmias can be categorized into two major classes; the first class consists of arrhythmias formed by a single irregular ECG signal, herein called morphological arrhythmia, the other type consists of arrhythmias formed by a set of irregular heartbeats, herein called rhythmic arrhythmias [18].

The main problem in the process of identifying and classifying arrhythmias ECGs is that an ECG signal can vary for each person, and sometimes different patients have separate ECG morphologies for the same disease [19]. Moreover, two various diseases could have approximately the same properties on an ECG signal [20]. These problems cause some difficulties in the issue of heart disease diagnosis [21].

Furthermore, the ECG records analysis is complicated for a human due to fatigue; an alternative way for automatic classification is computerization techniques [22]. For arrhythmia classification from the signal received by ECG device needed an automated system that can be divided into three main steps, as follows first: Pre-processing, next: Feature extraction and finally: Classification, as shown in Fig. 2 [23].



Fig. 1. A typical electrocardiogram signal [12].

ECG signals may contain several kinds of noises, which can affect the extraction of features used for classification; therefore, the pre-processing step is necessary for removing the noises [24]. Researchers have applied different preprocessing techniques for ECG classification. For noise removal, techniques such as low pass linear phase filter and linear phase high pass filters, etc., are used [25]. Some methods, such as median filter, linear phase high pass filter, and mean median filter are used baseline adjustment [26].

After the pre-processing step, extracting different ECG features then used as inputs to the classification model [27]. Feature extraction techniques used by researchers are discrete wavelet transform (DWT), continuous wavelet transform, discrete cosine transform (DCT), discrete Fourier transform, principal component analysis (PCA), Pan-Tompkins algorithm, and independent component analysis (ICA) [28].

When the set of features has been defined from the heartbeats, models can be built from these data using artificial intelligence algorithms from machine learning and data mining domains for arrhythmia heartbeat classification. The most popular techniques employed for this task and found in the literature are artificial neural networks (ANN), convolution neural network (CNN), DWT, support vector machines (SVM), decision tree (DT), Bayesian, Fuzzy, linear discriminate analysis (LDA), and k-nearest neighbors (KNN) [29].

Many surveys on ECG analysis and classification have been published. In Karpagachelvi [30] surveyed the most effective features for ECG analysis and classification as ECG. Features play a significant role in diagnosing most of the cardiac diseases. Nasehi and Pourghassem [31] provided a survey of variance types of seizure detection algorithms and their potential role in diagnostic. Various machinelearning approaches for ECG analysis and classification were reviewed in Roopa and Harish [23]. A comprehensive review was published in 2018, which includes a literature on ECG analysis mostly from the past decade, and most of the major aspects of ECG analysis were addressed such as preprocessing, denoising, feature extraction, and classification methods [16] (Previous works on ECG survey paper, Reviewer 2).



Fig. 2. General diagram of electrocardiogram classification.

The main purpose of this work is to review most of the common techniques that have been used mostly from the past 5 years. Moreover, the paper can be useful for the other researchers in identifying any issue in ECG classification and analyzing the research area as many aspects of the methods are addressed. (This section is the main purpose of the paper (reviewer 3)).

The section of this paper is ordered as follows: Section 2 contains Classification Techniques, and then Section 3 provides of Discussion, and finally, Section 4 presents the Conclusion.

2. CLASSIFICATION

A lot of pathological information about a patient's heart processes can be obtained by studying the ECG signal [32]. There are many approaches have been developed to classify heartbeats as it is essential for the detection of an arrhythmia [33]. Arrhythmias can be divided into two parts, which are life-threatening and non-life-threatening arrhythmias, a long-term ECG classification is required for the diagnosis of non-life-threatening arrhythmias that could be time-consuming and impractical, automatic algorithms exhibit a great aid. Consequently, automatic ECG classification of arrhythmias is one of the most worth studying in the world [34].

There are various classifiers that have been used for ECG classification task. In this paper, most common ECG classification methods are reviewed that were proposed since 2016–2020, these classification methods can be mainly clustered based on the classifiers into several categories such as ANNs, CNN, kNN, SVM, and DWT. All of the reviewed papers were accessed by three well-known publishers, which are IEEE, ScienceDirect, and Springer. (This section was wrote about why and how the authors select the papers for this state (Reviewer 2 and reviewer 3).

Different types of classification techniques are studied to classify ECG data under the variance features, as there are plenty of features in the ECG signal that can be extracted. Some of the classification methods are addressed below.

2.1. ANN

The ANN is an adaptive system with exciting features such as the ability to adapt, learn, and summarize; because ANN's parallel processing, self-organizing, fault-tolerant, and adaptive capabilities make it capable of solving many complex problems, ANN is also very accurate in the

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classification and prediction of outputs [35]. The neural network (NN) consists of the number of layers; the initial layer has an association as of the system input, and the end layer gives the output of the network [36]. NN s having hidden layers and sufficient neurons can be applied to any limited input-output mapping trouble [37]. The NN model consists of an input layer, the hidden layer, and output layer, as shown in Fig. 3 [38].

Many kinds of literature are published related to the ECG classification based on ANN. Below some of these new approach:

Chen *et al.* (2016) proposed a wavelet-based ANN (W-ANN) method that was based on the wavelet transform. The result illustrated that the W-ANN can provide lower computing time such that reduction time was 49% and cleaner ECG input signal. The method was implemented on the data MIT-BIH arrhythmia database and real ECG signal measurement [39].

Boussaa *et al.* (2016) presented the design of a cardiac pathologies detection system with high precision of calculation and decision, which consists of the mel-frequency coefficient cepstrum algorithms such as fingerprint extractor (or features) of the cardiac signal and the algorithms of ANN multilayer perceptron (MLP) type MLP classifier as fingerprints extracted into two classes: Normal or abnormal. The design and testing of the proposed system are performed on two types of data extracted from the MIT-BIH database: A learning base containing labeled data (ECG normal and abnormal) and another test base containing no-labeled data. The experimental results were shown that the proposed system combines the respective advantages of the descriptor mel-frequency cepstrum coefficient and the MLP classifier [40].



Fig. 3. Artificial neural network.

Savalia *et al.* (2017) distinguished between normal and abnormal ECG data using signal processing and NNs toolboxes in Matlab. Data, which were downloaded from an ECG database, PhysioBank, were used for learning the NN. The feature extraction method was also used to identify variance heart diseases such as bradycardia, tachycardia, firstdegree atrioventricular (AV), and second-degree AV. Since ECG signals were very noisy, signal processing techniques were applied to remove the noise contamination. The heart rate of each signal was calculated by finding the distance between R-R intervals of the signal. The QRS complex was used to detect AV blocks. The result showed that the algorithm strongly distinguished between normal and abnormal data as well as identifying the type of disease [41].

Wess et al. (2017) presented field-programmable gate array (FPGA)-based ECG arrhythmia detection using an ANN. The objective was to implement a NN-based machinelearning algorithm on FPGA to detect anomalies in ECG signals, with better performance and accuracy (ACC), compared to statistical methods. An implementation with PCA for feature reduction and a MLP for classification, proved superior to other algorithms. For implementation on FPGA, the effects of several parameters and simplification on performance, ACC, and power consumption were studied. Piecewise linear approximation for activation functions and fixed-point implementation was effective methods to reduce the number of needed resources. The resulting NN with 12 inputs and six neurons in the hidden layer, achieved, in spite of the simplifications, and the same overall ACC as simulations with floating-point number representation. An ACC of 99.82% was achieved on average for the MIT-BIH database [42].

Pandey *et al.* (2018) compared three different ANN models for classification normal and abnormal signals and using University of California, Irvine ECG 12 lead signal data. This work had used methods, namely, back propagation (BP) network, radial basis function (RBF) networks, and recurrent neural network (RNN). RNN models have shown better analysis results. ACC for testing classification was 83.1%. This result was better than some work, using the same database [43].

Sannino and Pietro (2018) proposed an approach based on a deep neural network (DNN) for the automatic classification of abnormal ECG beats, differentiated from normal ones. DNN was developed using the Tensor Flow framework, and it was composed of only seven hidden layers, with 5, 10, 30, 50, 30, 10, and 5 neurons, respectively. Comparisons were

made among the proposed model with 11 other well-known classifiers. The numerical results showed the effectiveness of the approach, especially in terms of ACC [44].

Debnath *et al.* (2019) proposed two schemes; at first, the QRS components have been extracted from the noisy ECG signal by rejecting the background noise. This was done using the Pan-Tompkins algorithm. The second task involved the calculation of heart rate and detection of tachycardia, bradycardia, asystole, and second-degree AV block from detected QRS peaks using MATLAB. The results showed that from detected QRS peaks, and arrhythmias, which are based on an increase or decrease in the number of QRS peaks, the absence of a QRS peak, could be diagnosed. The final task is to classify the heart abnormalities according to previously extracted features. The BP trained feed-forward NN has been selected for this research. Here, data used for the analysis of ECG signals are from the MIT database [45].

Abdalla et al. (2019) presented that approach was developed based on the non-linearity and nonstationary decomposition methods due to the nature of the ECG signal. Complete ensemble empirical mode decomposition with adaptive noise (CEEMDAN) was used to obtain intrinsic mode functions (IMFs). Established on those IMFs, four parameters have been computed to construct the feature vector. Average power, coefficient of dispersion, sample entropy, and singular values were calculated as parameters from the first six IMFs. Then, ANN was adopted to apply the feature vector using them and classify five different arrhythmia heartbeats downloaded from PhysioNet in the MIT-BIH database. The performance of the CEEMDAN and ANN was better than all existing methods, where the sensitivity (SEN) is 99.7%, specificity (SPE) is 99.9%, ACC is 99.9%, and receiver operating characteristic (ROC) is 01.0% [46].

2.2. Convolutional Neural Network (CNN)

The CNN is the most common technique to classify ECG, CNN is mainly composed of two parts, feature extraction and classification [47]. The section of feature extraction is responsible for extracting effective features from the ECG signals automatically, while the part of classification is in charge of classifying signals accurately by making use of the extracted features, as shown in Fig. 4 [48].

Many approaches are published the ECG classification based on CNN. Below some of these update works:

Zubair et al. (2016) proposed a model which was integrated into two main parts, feature extraction, and classification.



Fig. 4. Typical convolution neural network structure.

The model automatically remembers a suitable feature representation from raw ECG data and thus negates the need for hand-crafted features. Using small and patientspecific training data, the proposed classification system efficiently classified ECG beats into five different classes. ECG signal from 44 recordings of the MIT-BIH database is used to assess the classification performance, and the results demonstrate that the proposed approach achieves a significant classification ACC and superior computational efficiency than most of the state-of-the-art methods for ECG signal classification [49].

Yin *et al.* (2016) proposed a system that applies the impulse radio ultra-wideband radar data as additional information to assist the arrhythmia classification of ECG recordings in the slight motion state. Besides, this proposed system employs a cascaded CNN to achieve an integrated analysis of ECG recordings and radar data. The experiments are implemented in the Caffe platform, and the result reaches an ACC of 88.89% in the slight motion state. It turns out that this proposed system keeps a stable ACC of classification for normal and abnormal heartbeats in the slight motion state [50].

Oh *et al.* (2017) designed a nine-layer deep CNN DCNN to identify five different categories of heartbeats in ECG signals automatically. The test was applied in original and ECG signals that were derived from the available database. The set was artificially augmented for removing high-frequency noise. The CNN model was trained to utilize the augmented data and obtained an ACC of 93.47% and 94.03% in the identification of heartbeats in noise-free and original ECGs [51].

Zhai and Tin (2018) proposed an approach based on the CNN model with a different structure. The model was improved SEN, and positive predictive rate for S beats by more than 12.2% and 11.9%, respectively. The system provided a fully automatic tool and reliable to detect the arrhythmia heartbeat without any manual feature extraction or any expert assistant [52].

Zhang *et al.* (2019) introduced a new pattern recognition method in ECG data using DCNN. Different from past methods that utilized learn features or hand-crafted features from the raw signal domain, the proposed method was learned the features and classifiers from the time-frequency domain. First, the ECG wave signal was transformed into the time-frequency domain using the Short-Time Fourier Transform. Then, several scale-specific DCNN models were trained on ECG samples of a specific length. Eventually, an online decision fusion method was proposed to fuse decisions at different scales into a more accurate and stable one [53].

Wang (2020) proposed a novel approach for the automated atria fibrillation (AF) detection based DNN, which was built 11-layers. The network structure was combined using a modified Elman neural network (MENN) and CNN. Ten-Fold cross-validation was conducted to evaluate the classification performance of the model on the MIT-BIH AF database. The result confirmed that the model yielded excellent classification performance with the ACC, SEN, and SPE of 97.4%, 97.9%, and 97.1%, respectively [54].

Yao *et al.* (2020) designed model attention based on timeincremental CNN (ATI-CNN); a DNN model could obtain both spatial and temporal fusion of information from ECG signals using integrating CNN. The features were flexible input length, halved parameter amount as well as more than 90% computation reduction in real-time processing. The experiment result showed that ATI-CNN achieved an overall classification rate of 81.2% compared to VGGNET that is a classical 16-layer CNN, ATI-CNN achieved ACC increases of 7.7% in average, and up to 26.8% in detecting paroxysmal arrhythmias [55].

2.3. DWT

The DWT is used to recognize and diagnose the ECG signals and widely used in signal processing [56]. A perfect time resolution is the main advantage of DWT [57]. It provides good frequency resolution at low frequency and good resolution at high frequency [58]. The DWT can reveal the local characteristics of the input signal because of this great time and frequency localization ability [59].

Many kinds of literature are published related to the ECG classification based on DWT. Below some of these new approach:

Desai *et al.* (2015) described a machine learning-based approach for detecting five classes of ECG arrhythmia beats based on DWT features. Moreover, ICA was used to comprise dimensionality reduction. ANOVA approach was used to select significant features, and ten-fold crossvalidation was used to perform SVM. The experiment was conducted on MIT–BIH arrhythmia, which is grouped into five classes of arrhythmia beats, namely, non-ectopic (N), ventricular ectopic (V), supraventricular ectopic (S), fusion (F), and unknown (U). Using SVM quadratic kernel classified ECG features with an overall average ACC of 98.49% [60].

Saraswat (2016) explored diverse possibilities of the decomposition using the DWT method to classify Wolff Parkinson White Syndrome ECG signals. In this work, ECG signals are discretely sampled till the 5th resolution level of the decomposition tree using DWT with Daubechies wavelet of order 4 (db4), which helps in smoothing the feature more appropriate for detecting changes in signals. The MIT-BIH database was used for some experimental results [61].

Alickovic and Subasi (2016) noted that RF classifiers achieved superior performances compared to DT methods using ten-fold cross-validation for the ECG datasets. The results suggested that further significant developments in words of classification ACC could be accomplished by the proposed classification system. Accurate ECG signal classification was the major requirement for the detection of all arrhythmia types. Performances of the proposed system were evaluated on two different databases, namely, MIT-BIH database and St. Petersburg Institute of Cardiological Techniques 12-lead Arrhythmia Database. For the MIT-BIH database, the RF classifier generated an overall ACC of 99.33 % against 98.44 and 98.67 %, respectively. For St. Petersburg Institute of Cardiological Technics 12-lead Arrhythmia Database, RF classifier yielded a general ACC for the C4.5 and CART classifiers of 99.95% against 99.80% for both C4.5 and CART classifiers, respectively. The merged model with multiscale PCA de-noising, DWT, and RF classifier also achieves good performance for MIT-BIH database with the area under the ROC curve (area under the curve [AUC]) and F-measure equal to 0.999 and 0.993 and 1 and 0.999 for and St. Petersburg Institute of Cardiological Technics 12-lead Arrhythmia Database, respectively. The results demonstrated that the proposed system was able for reliable classification of ECG signals and to help the clinicians to make an accurate diagnosis of cardiovascular disorders (CVDs) [62].

Pan *et al.* (2017) proposed a comprehensive approach based on random forest techniques and discrete wavelet for arrhythmia diagnosis. Specifically, DWT was used to remove high-frequency noise and baseline drift, while DWT, autocorrelation, PCA, variances, and other mathematical methods are used to extract frequency-domain features, time-domain features, and morphology features. Moreover, an arrhythmia classification system was developed, and its availability was verified that the proposed scheme could significantly be used for guidance and reference in clinical arrhythmia automatic classification [63].

Sahoo (2017) proposed an improved algorithm to find QRS complex features based on the wavelet transform to classify four kids of ECG beats: Normal (N), left bundle branch block (LBBB), right bundle branch block (RBBB), and Paced beats (P); using NN and SVM classifier. Model performance was evaluated in terms of SEN, SPE, and ACC for 48-recorded ECG signals obtained from the MIT–BIH arrhythmia database. The proposed procedure achieved high detection efficiency with a low error rate of 0.42% when detecting the QRS compound. The classifier fixed its superiority with an average ACC of 96.67% and 98.39% in SVM and NN, respectively. The classification ACC of the SVM approach proves superior for the proposed method to that of the NN classifier with extracted parameters in detecting ECG arrhythmia beats [64].

Ceylan (2018) studied a model based on spared coefficients of the signals that were achieved by employing sparse representation algorithms and dictionary learning. The obtained coefficients were utilized in the weight update process of three different classification approaches, which were created using SVM, AdaBoost, and LDA algorithms. In the first step, the proposed Dictionary Learning (DL) based AdaBoost classifiers isolated the ECG signals. Then, the selected feature was applied to ECG signals, and six different feature subsets were obtained by DWT, T-test, Bhattacharyya, First Order Statistics (FOS), Wilcoxon test, and Entropy methods. The subscription of objects was used as a new dataset. The classification process is performed according to the proposed method, and satisfactory results are obtained. The best classification ACC was received at 99.75% using the proposed commercial-based terminology method called DL-AdaBoost-SVM for the subset of attributes obtained using the DWT and Wilcoxon test methods [65].

Tea and Vladan (2018) proposed a novel framework that combined the theory of compressive sensing and random forests to achieve reliable automatic cardiac arrhythmia detection. Moreover, it evaluated the characterization power of DCT, DWT, and FFT data transformations to extract significant features that can bring an additional boost to the classification performance. The experiments conducted on the MIT-BIH benchmark arrhythmia database, the result demonstrated that DWT based features exhibit better returns compared to the feature extraction technique for a relatively small number of random projected coefficients. Furthermore, due to its low-complexity, the proposed model could be implemented for practical applications of real-time ECG monitoring [66].

Zhang et al. (2019) proposed a lightweight approach to classify five types of cardiac arrhythmia; namely, normal beat (N), premature ventricular contraction (PVC) (V), atria premature contraction (APC) (A), RBBB beat (R), and LBBB beat (L). The mixed method of frequency analysis and Shannon entropy was applied to extract appropriate statistical features. The information gain criterion was manipulated for selecting features. The selected features were then fed to the input of Random Forest, KNN, and J48 for classification. To evaluate classification performance, tenfold cross-validation was used to verify the effectiveness of our method. Experimental results showed that the Random Forest classifier demonstrates significant performance with the SPE of 99.5%, the highest SEN of 98.1%, and the ACC of 98.08%, outperforming other representative approaches for automated cardiac arrhythmia classification [67].

Kora et al. (2019) showed that an algorithm to detect atrial fibrillation (AF) in the ECG signal is developed. For correct detection of AF, pre-processing and feature extraction of the ECG signal shall be performed before it detects AF. After considering the ECG signal from the database, in the preprocessing stage, denoising of the ECG signal is carried out to obtain a clean ECG signal. After pre-processing, before feature extraction, R peak detection is carried out for the signal. Since R peak has the highest amplitude, and therefore, it is detected in the first round, and subsequently location of other peaks of the ECG signals is performed. After completing, pre-processing and feature extraction using DWT applied based on inverted T wave logic and ST-segment elevation. Our classification algorithm was demonstrated to successfully acquire, analyze, and interpret ECGs for the presence of AF, indicating its potential to support m-Health diagnosis, monitoring, and management of therapy in AF patients [68].

2.4. SVM

SVM is a learning algorithm that has many good properties. It is associated with data analysis and recognizes the pattern. SVM uses a linear discriminate function for classification; however, non-linear classification can also be done if a non-linear kernel is used [69]. SVM performs well in real-time situations, robust, easy to understand. While compared to other classifiers [30]. A classification task typically requires the knowledge about the data to be classified; hence, the classifier must be trained before classifying any data [70]. One of the main advantages of the SVM classifier is that it automatically finds the support vectors for better classification [71]. Majorly, in every case the performance of SVM depends on the affected kernel function selection [72].

Many types of research are published in the ECG classification based on the SVM. Below some of these recent studies:

Elhaj et al. (2016) investigated a combination of linear and non-linear features to improve the classification of ECG data. In the study, five types of beat classes of arrhythmia as recommended by the Association for Advancement of Medical Instrumentation are analyzed: Non-ectopic beats (N), supra-ventricular ectopic beats (S), ventricular ectopic beats (V), fusion beats (F), and unclassifiable and paced beats (U). The characterization ability of non-linear features such as high order statistics and cumulants and non-linear feature reduction methods such as ICA is combined with linear features, namely, the PCA of DWT coefficients. The features are tested for their ability to differentiate different classes of data using different classifiers, namely, the SVM and NN methods, with tenfold cross-validation. This method can classify the N, S, V, F, and U arrhythmia classes with high ACC (98.91%) using a combined SVM and RBF method [73].

Arjunan (2016) reported that statistics features could be useful for categorizing the ECG signals. Like the first, the signal has been passed from the de-noising process as a pre-processing. Then, the following statistics features such that mean, variance, standard deviation, and skewness are extracted from the signal. SVM was implemented to classify the ECG signal into two categories; normal or abnormal. The results show that the system classifies the given ECG signal with 90% SEN and SPE [74].

Smíšek *et al.* (2017) proposed method for automatic ECG classification to four classes (normal rhythm [N], AF [A], another rhythm [O], and noisy records [P]). The SVM approach was involved in the two different stages in the model. In the first stage, SVM was used to extract the global

features from the entire ECG signal. In the second stage, the features from the previous step were used to train the second SVM classifier. The cross-validation technique was used to evaluate both classifiers. The result showed that in Phase II of challenge, the total F1 score of the method was 0.81 and 0.84 within the hidden challenge dataset and training set, respectively [75].

Wu et al. (2017) developed a system for identifying excessive alcohol consumption. Three sensors were used to acquire signals regarding (ECG), intoxilyzers, and photoplethysmograph (PPG). Intoxilyzers were used to know alcohol consumption levels of participants before and after drinking. The signals were pre-processed, segmented, and subjected to feature extraction using specific algorithms to produce ECG and PPG training and test data. Using the ECG, PPG, and alcohol consumption data, the developed model was fast and accurate for the identification scheme using the SVM algorithm. Using the training data for training and the test data were applied to comfort the recognition performance of the trained SVMs. The identification performance of the proposed classifiers achieved 95% on average. In the approach, different feature combinations were tested to select the optimum technological configuration. Because the PPG and ECG features produce identical classification performance and the PPG features were more convenient to acquire, the technical setting based on PPG is preferable for developing smart and wearable devices for the identification of driving under the influence [76].

Venkatesan *et al.* (2018), ECG signal pre-processing and SVM -based arrhythmic beat classification is performed to categorize into normal and abnormal subjects. In ECG signal pre-processing, a delayed error normalized LMS adaptive filter is used to achieve high speed and low latency design with less computational elements. Since the signal processing technique is developed for distant healthcare systems, white noise removal is mainly focused. DWT is applied to the pre-processed signal for HRV feature extraction, and machine-learning techniques are used for performing arrhythmic beat classification. In this paper, the SVM classifier and other popular classifiers have been used on noise removed feature extracted signal for beat classification. The results show that the SVM classifier performs better than additional machine learning-based classifiers [77].

Liu *et al.* (2019) proposed an ECG arrhythmia classification algorithm based on CNN. They compared the CNN models with combining linear discriminant analysis (LDA) and SVM. All cardiac arrhythmia beats are derived from the MIT-BIH Arrhythmia Database, which was classed into five groups according to the standard developed by the Association for the Advancement of Medical Instrumentation (AAMI). The training set and the testing set come from different people, and the correction of classification is >90% [78].

2.5. KNN

The KNN algorithm is a simple machine-learning algorithm compared to similar machine learning approaches [79]. Most of the machine-learning algorithms work on the KNN algorithm [80]. KNN classifier is an instance-based learning method, which stores all training sample vectors [81]. It is a very simple and effective method, especially for highdimensional problems [82]. It classifies the new unknown test samples based on similar training samples [83]. The similarity measure is usually the Euclidean distance [84]. K-NN classifier was based on grouping of closest training points of data in the considered feature space. The majority of voters do the cluster to the nearest neighbor points [85].

Many approaches are published the ECG classification based on KNN. Below some of these new works:

Faziludeen and Sankaran (2016) presented a method for automatic ECG classification into two classes: Normal and PVC. The Evidential K-Nearest Neighbors (EKNN) was based on the Dempster Shafer Theory for classifying the ECG beats. RR interval features were used. The analysis was performed on the MIT-BIH database. The performance of EKNN was compared with the traditional KNN (maximum voting) approach. The effect of training data size was assessed using training sets of varying sizes. The EKNN based classification system was shown to out perform the KNN based classification system consistently [86].

Bouaziz *et al.* (2018) implemented an automatic ECG heartbeats classifier based on KNN. The segmentation of ECG signals has been performed by DWT. The considered categories of beats are normal (N), PVC, APC, RBBB, and LBBB. The validation of the presented KNN based classifier has been achieved using ECG data from MIT-BIH arrhythmia database. They have obtained the excellent classification performances, in terms of the calculated values of the SPE and the SEN of the classification rate, which is equal to 98, 71% [87].

Khatibi and Rabinezhadsadatmahaleh (2019), a novel feature engineering method, was proposed based on deep learning and K-NNs. The features extracted were classified with

different classifiers such as DTs, SVMs with different kernels, and random forests. This method has good performance for beat classification and achieves the average ACC of 99.77%, AUC of 99.99%, precision of 99.75%, and recall of 99.30% using fivefold Cross-Validation strategy. The main advantage of the proposed method was its low computational time compared to training deep learning models from scratch and its high ACC compared to the traditional machine learning models. The strength and suitability of the proposed method for feature extraction are shown by the high balance between SEN and SPE [88].

3. DISCUSSION

The ECG classification, which shows the status of the heart and the cardiovascular condition, is essential to improve the patient's living quality. The main purpose of this work is to review the main techniques of ECG signal classification. In general, any structure of ECG classification can be divided into four stages. The first one is a preprocessing step, which is a crucial step in the ECG signal classification. For that reason, most well-known techniques are reviewed in this paper. The idea of using the preprocessing step and the combination of preprocessing techniques is to improve the performances of the model. The second step is extracting the most relevant information from the ECG signal, which represents the heart status. The step is called a feature extraction step. There is a vital challenge to extract efficient information that can be discriminated based on the variance status of the ECG signal. The success rate of the model can evaluate whether the feature contains valuable knowledge of the signal or not. The third step is named as the feature selection step. Time execution of the model is a crucial part and can be reduced using optimal features among the feature spaces. Many techniques have been adopted for reducing the dimensionality of the features. Some of the methods have been inspired by nature and the others, working based on the mathematical rules. The primarily focused step is selecting a machine-learning algorithm to classify the ECG features. Plenty of approaches has been used for this purpose. Most of the classifier methods are fed by the features, but CNN is supplied using the raw signal as CNN is a feature-less technique. ANN, CNN, DWT, KNN, and SVM are reviewed. All reviewed articles are downloaded from three trusted sources, IEEE, ScienceDirect, and Springer for 2015–2020. Tables 1-5 show the summarization of all the reviewed articles in term of what kind of machine-learning were used, how the methods were effective to the ECG

TABLE 1: Heartbeat methods classification based on ANN							
Artificial neural networks							
Author (year)	Dataset	Purpose	Methods	Result	Remarks		
Chen <i>et al.</i> (2016)	MIT-BIH arrhythmia dataset	Reduce the computing time by a simple method	Wavelet Artificial Neural Network (W-ANN)	The average computing time can be reduced by 49%	Use a mobile real-time applications to classify ECG		
Boussee <i>et al.</i> (2016)	MIT-BIH arrhythmia dataset	Record, proceed, and classify ECG signal	Mel Frequency Coefficient Cepstrum (MFCC)+ANN	Available a robust and quick classification system	Build a system to classify ECG by a combination of signal processing algorithms		
Savalia <i>et al.</i> (2017)	MIT/BIH Normal Sinus Database and MIT-BIH arrhythmia dataset	To distinguish normal and abnormal ECG	ANN	Accuracy=86%	Abnormal ECG is used to identify specific heart diseases		
Wess <i>et al.</i> (2017)	MIT-BIH arrhythmia dataset	To present FPGA- based ECG arrhythmia detection	PCA+ANN	Accuracy=99.82%	Increased the number of inputs, hidden layer, and fixed point		
Pandey <i>et al.</i> (2018)	UCI arrhythmia dataset	Early and right identification of cardiac disease	RNN, RBF and BPA	Accuracy RNN=83.05% RBF=75.25% BPA=74.35%	Accuracy of RNN is better than two ANN models		
Sannino and Pietro (2018)	MIT-BIH arrhythmia dataset	The automatic recognition of abnormal	DNN	Accuracy=99.68%	The model is competitive in sensitivity and specificity		
Debnath <i>et al.</i> (2019)	MIT-BIH arrhythmia dataset	Analyze and Predict heart abnormality	ANN	Accuracy Normal=97.46% Bradycardia=87.20% Tachycardia=99.97% Block=66.72%	Input noisy ECG signals		
Abdalla <i>et al.</i> (2019)	MIT-BIH arrhythmia dataset	Distinguish between different types of ECG arrhythmia	CEEMDAN+ANN	Accuracy=99.9%	The performance of the CEEMDAN and ANN is better than all existing methods		

Lana Abdulrazaq Abdullah and Muzhit Shaban Al-Ani: A Review of ECG Signal Classification

TABLE 2: Heartbeat methods classification based on CNN

Convolutional neural network						
Author (year)	Dataset	Purpose	Methods	Result	Remarks	
Zubair <i>et al.</i> (2016)	MIT-BIH arrhythmia database	Proposed learns features from raw ECG	1D-CNN	Accuracy=92.7%	The model avoids the need for hand-crafted features	
Yin <i>et al</i> . (2016)	Data is built on ECG sensor chip BMD101 and Bluetooth module	Monitoring and classifying ECG signals and radar signals	Cascade CNN	Accuracy=88.89%	The system can achieve stable performance in the slight motion state	
Oh <i>et al</i> . (2017)	MIT-BIH arrhythmia database	Identified automatically five different categories of ECG	9-layers CNN	Accuracy With noise=94.03% Without noise=93.47%	Generated synthetic data to overcome imbalance problems	
Zhai and Tin (2018)	MIT-BIH arrhythmia database	Implemented model on portable device for long- term monitoring	CNN	Accuracy>97%	The model doesn't need manual feature extraction or expert assistant	
Zhang <i>et al.</i> (2019)	Synthetic and real- world ECG datasets	Proposed learns features and classifiers from the time-frequency domain	DCNN	Accuracy=99%	The model can integrated into a portable ECG monitor with limited resources	
Wang (2020)	MIT-BIH AF dataset	Proposed approach for automated AF detection	CNN+MENN	Accuracy=97.4%	The model has great potential to assist physicians and reduce mortality	
Yao <i>et al</i> . (2020)	China Physiological Signal Challenge 2018 database	Classify varied-length ECG signals	Attention-based time-incremental (ATI)-CNN	Accuracy=81.2%	The model compares with VGGNet, increases the accuracy	

TABLE 3: Heartbeat methods classification based on DWT

Discrete wavelet transforms						
Author (year)	Dataset	Purpose	Methods	Result	Remarks	
Desai <i>et al.</i> (2015)	MIT-BIH arrhythmia dataset	Detected five classes of ECG arrhythmia	DWT+ICA+SVM	Accuracy =98.49%	efficient system in healthcare diagnosis	
Saraswat <i>et al.</i> (2016)	MIT-BIH arrhythmia dataset	Presented a clear difference between normal and abnormal ECG	DWT	Provide min and max values of normal and abnormal ECG.	detecting changes in signals leading to smooth the feature	
Alickovic and Subasi (2016)	MIT-BIH arrhythmia and StPetersburg Institute of Cardiological Technics Arrhythmia Database	Automated system for the classification of ECG	DWT+C4.5+CART	Accuracy C4.5=99.95% CART=99-80%	Efficient system for cardiac arrhythmia detection	
Pan <i>et</i> <i>al</i> .(2017)	MIT-BIH arrhythmia dataset	Developed system for clinical arrhythmia classification	DWT+random forest	Accuracy=99.77%	The system improves classification accuracy and speed	
Sahoo <i>et al.</i> (2017)	MIT-BIH arrhythmia dataset	Improved algorithm to detect QRS complex features to classify four types of ECG	Multiresolution WT +NN+SVM	Accuracy NN=96.67% SVM=98.39%	Extracted features are acceptable for classifying ECG by SVM	
Ceylan (2018)	MIT-BIH arrhythmia dataset	system for signal compression, noise elimination, and classification	DWT+AdaBoost+ SVM+LDA+DL	Accuracy > 99%	The best classification accuracy was obtained by (DL-AdaBoost – SVM)	
Tea and Vladan (2018)	MIT-BIH benchmark arrhythmia dataset	Monitor ECG in real –time	FFT+DCT+DWT +random forests	Accuracy=97.33%	DWT provides the best performance in comparison with FFT and DCT	
Zhang <i>et al.</i> (2019)	MIT-BIH arrhythmia dataset	Diagnosis of lowecost wearable ECG device	DWT+RF+KNN+J48	Accuracy=98.08%	Reduce the computational cost and improves the classification efficiency.	
Kora <i>et al</i> . (2019)	MIT-BIH arrhythmia dataset	Detect Atrial Fibrillation in the ECG signal	DWT+KNN+SVM	Accuracy DWT+SVM=94.07% DWT+KNN= 99.5%	DWT represent the essential characteristics of the ECG	

Lana Abdulrazaq Abdullah and Muzhit Shaban Al-Ani: A Review of ECG Signal Classification

TABLE 4: Heartbeat methods classification based on SVM

Support vector machines						
Author (year)	Remarks					
Elhaj <i>et al</i> .(2016)	MIT-BIH arrhythmia database	Classifying ECG signal with high accuracy	PCA+DWT+ICA+ HOS+NN+SVM-RBF	Accuracy SVM-RBF=98.91% NN=98.90%	Both classifiers provide equal average accuracy, sensitivity, and specificity	
Arjunan (2016)	MIT-BIH arrhythmia database	Categorize ECG by an automated system	SVM	Accuracy=90%	Mean, variance, standard deviation, and skewness are used for feature extraction	
Smíšek <i>et al.</i> (2017)	Hidden dataset of 2017 PhysioNet/ CinC Challenge	An advanced method for automatic classification ECG	SVM-RBF	F1-measure=0.81	Quite high performance was achieved even for low number in training set	
Wu <i>et al.</i> (2017)	Collect data by sensors.	Recognize drunk driving by ECG and PPG	SVM	Accuracy=95%	The smart and wearable sensing devices offer right solution for drunk driving	
Venkatesan <i>et al.</i> (2018)	MIT-BIH arrhythmia database.	Classifier with low computational complexity	SVM	Accuracy=96%	SVM is better than various classification techniques	
Liu <i>et al</i> . (2019)	MIT-BIH arrhythmia database.	Robust and efficient model to achieve a real- time analysis ECG	SVM+CNN+LDA	Accuracy >90%	Sometimes, do not need to extract complex features of ECG	

TABLE 5: Heartbeat methods classification based on KNN

K- nearest neighbors						
Author (year)	Dataset	Purpose	Methods	Result	Remarks	
Faziludeen and Sankaran(2016)	MIT-BIH arrhythmia database	Classify ECG beat into two classes	KNN+EKNN	Lower error rates	Increase in training size is shown to lower the error rates	
Bouaziz <i>et al</i> . (2018)	MIT-BIH arrhythmia database	Implement an automatic ECG heartbeats classifier	KNN	Accuracy=98.71%	KNN an important and significant tool for ECG recognition	
Khatibi and Rabinezhadsadatmahaleh (2019)	MIT-BIH arrhythmia database	Classify ECG for arrhythmia detection	CNN+DT+S VM+RF+K-NNs	Accuracy=99.77%	The method is low computational time	

classification and which kind of ECG datasets were used. Some important points in the ECG classification are observed and highlighted in the below:

According to the previous works based on the ANN algorithm for heartbeat classification, ANN is trained using the polyspectrum patterns and features extracted from the higher-order spectral analysis of normal and abnormal ECG signal. ANN is used as a classifier to help knowledge management and decision-making system to improve classification ACC. The result shows that ANN with PCA obtains lowest error rate to classify the ECG signal. The performance of the CEEMDAN and ANN is better than all higher than all existing and previous algorithms (Table 1). (The main point are extracted from ANN [Reviewer 1 and 2 and 3]).

CNN is straight forward to apply as the CNN is a features less techniques. Hence, the researcher does not concern about the feature that means any handcraft feature does not require in the CNN model. 1 D and 2 D of CNN have been adopted, According to the observed result, 1 D CNN outperformed of the 2D CNN. Moreover, the 1D CNN is less complex compare to the 2 D CNN in term of computational steps. CNN also can be integrated with MENN to improve the classification ACC (Table 2). (Roles CNN in ECG classification [Reviewer 1 and 2 and 3]).

DWT is applied on each heartbeat to obtain the morphological features. It provides better time and frequency resolution of ECG signal. DWT shows the powerful tool for ECG classification and it is straight forward tool to implantation. Moreover, DWT is an assisting the clinicians for making an accurate diagnosis of CVDs. Based on the summarization of some works on DWT, the integration DWT model with random forest can achieve 99.77% ACC (Table 3) (The main notes about DWT [Reviewer 1 and 2 and 3]).

SVM (SVM) is widely used for pattern recognition. SVM model with a weighted kernel function method significantly

recognizes the Q wave, R wave, and S wave in the input ECG signal to categorize the heartbeat. SVM is also the powerful tool to ECG classification; however, the performance CNN has outperformed of the SVM. Moreover, the time consumption of implementing SVM is higher than KNN model and smaller than the CNN model. SVM-RBF classifier classifies 95% of the given ECG signal correctly with simple statistical features Table4. (The contributions of SVM [Reviewer 1 and 2 and 3]).

The lowest computational rate for diagnosing arrhythmia can be achieved by applying KNN as the KNN algorithm does not require the training stage. The role of the handcraft features is a vital subject to the KNN model as long as the dimensional of the obtained features is low because the KNN model works based on the distance. Time domain and frequency domain features are applied to KNN classifier for ECG classification which is simpler than other machinelearning approaches (Table 5). (The main roles of kNN in ECG classification [Reviewer 1 and 2 and 3]).

4. CONCLUSION

Classification of ECG signals is acting an important role in recognizing normal and abnormal heartbeat. Increasing the ACC of ECG classification is a challenging problem. It has been interested in more than a decade; for this reason, many approaches have been developed. In this paper, most recent approaches are reviewed in terms of some aspects such as method, dataset, contribution, and success rate. The table (CNN) summarizes variance approaches in ECG signal analysis. We suggest using a hybrid model based on CNN with long- and short-term memory (LSTM). The CNN part can extract the features from the raw signal which can be a temporal features based on how many convolution layers we will used, and LSTM can learn the pattern in the temporal feature as the LSTM is more suitable to time series features. Then, the model can predict unknown ECG signals. We will tune filters in the CNN model and layers in the LSTM model to increase the classification rate. (Explain how use CNN+LSTM [Reviewer 3]).

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- UHD Journal of Science and Technology | Jul 2020 | Vol 4 | Issue 1

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